

BRAIN COMMUNICATIONS

State-dependent signatures of anti-*N*-methyl-D-aspartate receptor encephalitis

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Traditional static functional connectivity analyses have shown distinct functional network alterations in patients with anti-*N*-methyl-D-aspartate receptor encephalitis. Here, we use a dynamic functional connectivity approach that increases the temporal resolution of connectivity analyses from minutes to seconds. We hereby explore the spatiotemporal variability of large-scale brain network activity in anti-*N*-methyl-D-aspartate receptor encephalitis and assess the discriminatory power of functional brain states in a supervised classification approach. We included resting-state functional magnetic resonance imaging data from 57 patients and 61 controls to extract four discrete connectivity states and assess state-wise group differences in functional connectivity, dwell time, transition frequency, fraction time and occurrence rate. Additionally, for each state, logistic regression models with embedded feature selection were trained to predict group status in a leave-one-out cross-validation scheme. Compared to controls, patients exhibited diverging dynamic functional connectivity patterns in three out of four states mainly encompassing the default-mode network and frontal areas. This was accompanied by a characteristic shift in the dwell time pattern and higher volatility of state transitions in patients. Moreover, dynamic functional connectivity measures were associated with disease severity and positive and negative schizophrenia-like symptoms. Predictive power was highest in dynamic functional connectivity models and outperformed static analyses, reaching up to 78.6% classification accuracy. By applying time-resolved analyses, we disentangle state-specific functional connectivity impairments and characteristic changes in temporal dynamics not detected in static analyses, offering new perspectives on the functional reorganization underlying anti-*N*-methyl-D-aspartate receptor encephalitis. Finally, the correlation of dynamic functional connectivity measures with disease symptoms and severity demonstrates a clinical relevance of spatiotemporal connectivity dynamics in anti-*N*-methyl-D-aspartate receptor encephalitis.

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Abbreviations: AG = angular gyrus; CB = cerebellar; dATT = dorsal attention network; DMN = default-mode network; FC = functional connectivity; FDR = false discovery rate; FNC = functional network connectivity; FPN = fronto-parietal network;

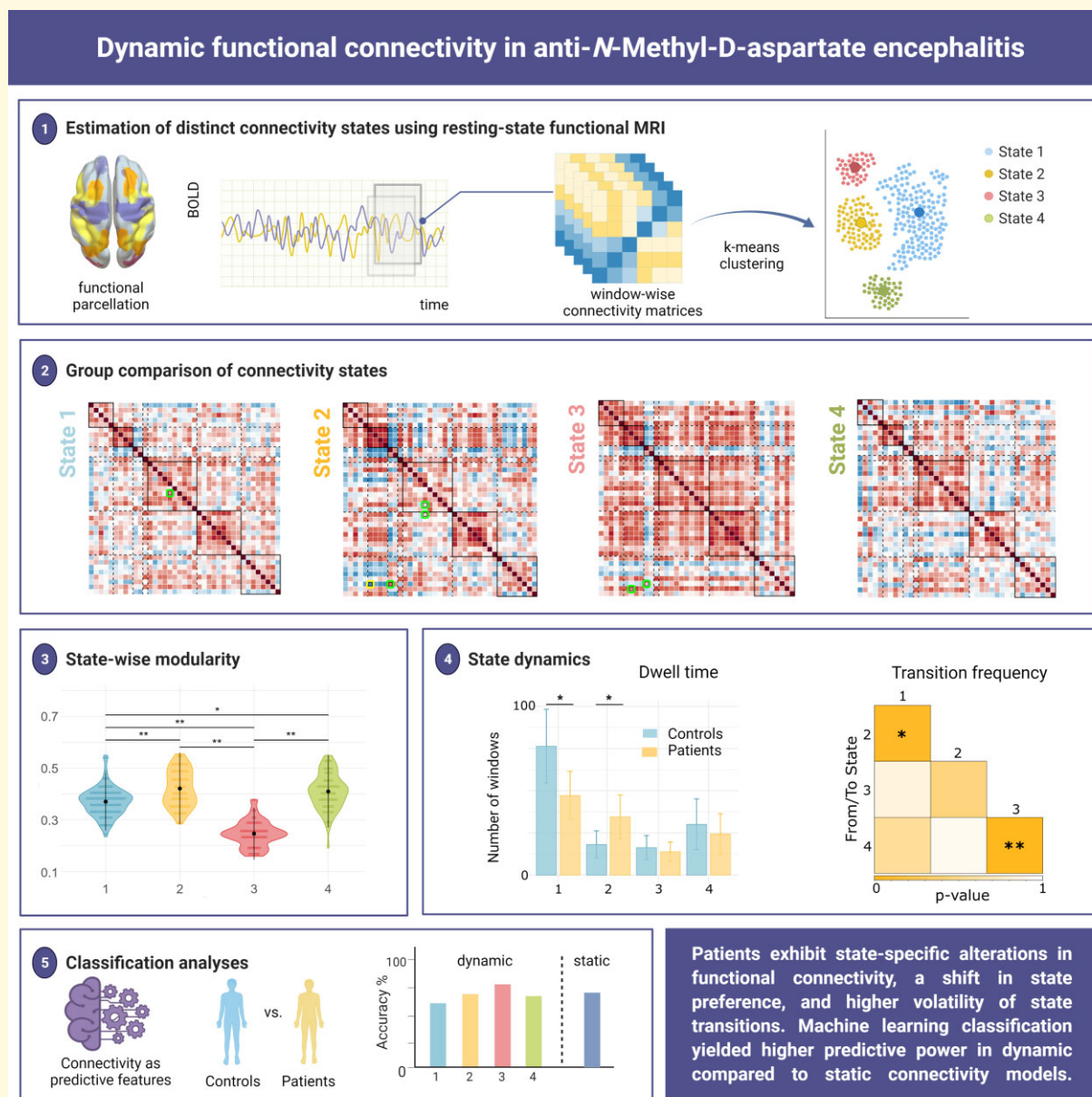
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HC = healthy controls; HPC = hippocampus; IFG = inferior frontal gyrus; LOOCV = leave-one-out cross-validation; mPFC = medial prefrontal cortex; MPRAGE = Magnetization-Prepared Rapid Gradient Echo; mRS = modified Rankin scale; OFG = orbito-frontal gyrus; PC = principal component; PHG = parahippocampal gyrus; POS = parieto-occipital gyrus; prim. Visual = primary visual cortex; rs-fMRI = resting-state functional MRI; SB = subcortical; SFG = superior frontal gyrus; SM = sensorimotor; SMA = supplementary motor area; STG = superior temporal gyrus; TE = echo time; TPOJ = temporo-parieto-occipital junction; TR = repetition time

Graphical Abstract



Introduction

Anti-*N*-methyl-D-aspartate (NMDA) receptor encephalitis is a severe autoimmune disorder of the CNS caused by antibodies targeting the NR1 subunit of the NMDA receptor.¹ The disease is characterized by a complex neuropsychiatric syndrome with delusions, hallucinations, movement abnormalities, autonomic dysfunction, decreased levels of

consciousness and cognitive dysfunction, e.g. deficits of executive control and memory.^{1–6}

Despite the severe disease course, routine clinical MRI reveals no abnormalities in 50–80% of patients.^{5,7} In contrast, functional connectivity (FC) is disrupted in distinct functional networks, including medial-temporal, fronto-parietal and visual networks.⁸ Specifically, hippocampal connectivity with medial prefrontal regions of the default-mode network

(DMN) is significantly impaired, and these alterations are associated with the severity of memory impairment. Moreover, disruption of fronto-parietal and ventral attention networks correlates with positive and negative schizophrenia-like symptoms.^{3,8} These traditional resting-state FC analyses have thus contributed to reveal the mechanisms underlying clinical symptoms in anti-NMDA receptor encephalitis by assessing the coherence of brain activity between distinct regions. However, traditional FC analyses are ‘static’ in the sense that blood-oxygen-level dependent time series are averaged across a scan with duration of several minutes.

Yet, the brain is a complex dynamic system in which the strength and spatial organization of connectivity patterns can change within seconds, resulting in multiple spatiotemporal organization patterns during one MRI scan.^{9–11} ‘Dynamic’ FC approaches capture these changes of functional brain organization and allow for the investigation of temporal properties, i.e. identification of distinct connectivity states and analysis of transition trajectories between these states—alterations of which may vary with the disease.⁹ Indeed, recent studies report intriguing evidence that dynamic FC analyses enable a better characterization of network alterations in psychiatric and neurological diseases compared to static FC approaches.¹⁰ Therefore, dynamic FC measures are increasingly understood as meaningful attributes to describe different disease phenotypes, e.g. in schizophrenia, major depression, stroke and Alzheimer’s disease.^{12–15}

One common method to analyse dynamic FC applies a clustering algorithm to obtain distinct functional brain states, which are defined as time-varying, but recurrent patterns of FC.¹⁶ This approach provides a specifically promising tool for disentangling the dynamic network changes underlying the diverse neuropsychiatric symptoms in anti-NMDA receptor encephalitis. Here, we used this approach to (i) investigate the spatiotemporal properties of brain states in a large sample of patients with anti-NMDA receptor encephalitis and healthy controls (HC); (ii) explore the relationship between state dynamics, disease severity and duration and psychiatric symptoms and (iii) evaluate the potential of each brain state to discriminate between patients and controls using a supervised machine learning approach.

Materials and methods

Participants

For this study, 57 patients with anti-NMDA receptor encephalitis (female: 50, median age: 25.00 ± 14.50 years) were recruited from the Department of Neurology at Charité-Universitätsmedizin Berlin. The diagnosis was based on clinical presentation and detection of IgG NMDA receptor antibodies in the cerebrospinal fluid. Patients were in the post-acute disease stage, with a median

of 2.43 years (± 2.95) between disease onset and MRI data acquisition. The median disease duration, i.e. days spent in hospitalization, was 63 days (± 56.50 , $N = 52$). Disease severity at the time of scan was assessed based on the modified Rankin scale (mRS; median mRS: 1.00 ± 1.00 , $N = 55$). The control group consisted of 61 age- and sex-matched healthy participants (female: 54, median age: 26.00 ± 11.00 years) with no history of neurological or psychiatric disease. Clinical and demographic characteristics are summarized in [Supplementary Table 1](#). All participants gave written informed consent, and the study was approved by the local ethics committee.

MRI data acquisition

Structural and functional MRI data were acquired at the Berlin Center for Advanced Neuroimaging at Charité-Universitätsmedizin Berlin using a 20-channel head coil and a 3 T Trim Trio scanner (Siemens, Erlangen, Germany). For resting-state functional MRI (rs-fMRI), we employed an echoplanar imaging sequence [repetition time (TR) = 2.25 s, echo time = 30 ms, 260 volumes, voxel size = $3.4 \text{ mm} \times 3.4 \text{ mm} \times 3.4 \text{ mm}$]. High-resolution T₁-weighted structural scans were collected using a Magnetization-Prepared RAPid Gradient Echo sequence (MPRAGE; $1 \text{ mm} \times 1 \text{ mm} \times 1 \text{ mm}$).

MRI data analysis

Our processing pipeline followed the procedure of recent related work.¹⁶ Preprocessing of rs-fMRI scans included discarding the first five volumes to account for equilibration effects, slice time correction, realignment to the first volume, spatial normalization to MNI space (voxel size $2 \text{ mm} \times 2 \text{ mm} \times 2 \text{ mm}$) and spatial smoothing with a 6-mm full width at half maximum smoothing kernel using the CONN Toolbox (<https://web.conn-toolbox.org/>).

Group-independent component analysis

To perform group-independent component analysis and dynamic functional network analysis, we applied the GroupICA fMRI toolbox (GIFT, <http://mialab.mrn.org/software/gift/index.html>). For each participant, 255 time points were first decomposed into 150 temporally independent principle components (PCs) and subsequently into 100 independent PCs using the *Infomax* algorithm.¹⁷ This procedure was repeated 20 times in ICASSO to estimate the reliability and ensure the stability of the decomposition.¹⁸ For back-reconstruction of individual time courses and spatial maps, *gig-ica* (integrated in the GIFT Toolbox) was applied to the data.¹⁹ The resulting 100 independent components were individually rated as signal or noise by three independent raters (N.v.S., J.H., C.F.). In total, 39 components were assigned to functional networks based on the labels proposed by Thomas Yeo *et al.*²⁰ For cerebellar

(CB) and subcortical (SB) components, two distinct networks were added. This yielded a total of seven functional resting-state networks including sensorimotor (SM), visual (VIS), SB, CB, DMN, dorsal attention and fronto-parietal network (FPN). [Supplementary Fig. 1](#) shows all functional networks and [Supplementary Table 2](#) contains peak values and coordinates for all components. Finally, we applied additional processing steps including linear, quadratic and cubic detrending, motion regression (12 motion parameters) to reduce motion-related artefacts, high-frequency cut-off at 15 Hz, despiking (identified as framewise displacement > 0.5 mm) and interpolation of time courses using a third-order spline fit.

Static functional network connectivity analysis

To compare the dynamic FC results with conventional ‘static’ FC, we calculated the average pairwise connectivity between all component pairs across the resting-state scan using Pearson’s correlation coefficient r for each subject. Subsequently, age, sex and motion parameters were regressed out, and Fisher z -transformation was applied.

Dynamic functional network connectivity analysis

In order to obtain FC dynamics, FC between all component pairs was calculated over consecutive windowed segments of the time courses (i.e. sliding windows) using a window of 30TR length ($\hat{=}$ 67.5 s) that shifted in steps of 1TR ($\hat{=}$ 2.25 s). After the correlation matrix was computed on each window (i.e. 225 39×39 matrices per participant), Fisher z -transformation was applied and age, sex and motion parameters were regressed out as nuisance variables. Subsequently, matrices of each participant were concatenated, and k -means clustering was applied with $k=4$ according to the elbow criterion (see [Supplementary Fig. 2](#)). Thus, each window was assigned to one of the four clusters representing discrete network FC states.¹⁶ Squared Euclidean distance was applied for clustering, and the process was repeated 100 times to avoid convergence on local minima.

Statistical analysis for group differences in static and dynamic functional network connectivity

For a global characterization of the static and the state-wise correlation matrices, modularity (as a measure of functional network segregation) and absolute mean connectivity (referred to as ‘overall connectivity’) were calculated.^{21,22} In the static FC analysis, both measures were calculated on each subject’s connectivity matrix and subsequent group comparison was performed using a non-parametric t -test as applied in Glerean *et al.*²³ In the dynamic FC analysis,

modularity and absolute mean connectivity were calculated for all windows in each state and averaged for each subject. Subsequently, a two-way ANOVA was conducted to estimate group- and state-wise effects as well as their interaction. For *post hoc* analysis, a Kruskal–Wallis test was performed.

Next, we assessed group differences in FC between all component pairs for the static and the dynamic functional network analysis with respect to connectivity strength with a non-parametric t -test. For the dynamic FC analysis, group differences were evaluated for each state separately.

Statistical analysis for state dynamics

Besides the analysis of state-dependent connectivity patterns, estimation of time-varying FC provides the opportunity to capture dynamic metrics. Here, four commonly used metrics were calculated: (i) dwell time (i.e. average number of windows a participant spends in a particular state), (ii) transition frequency (i.e. a participant’s number of transitions between each pair of states), (iii) fraction time (i.e. percentage of windows spent in a state) and (iv) state occurrence rate (i.e. number of participants that entered the state over the course of the scan).^{12,15} Group differences in occurrence rates were estimated using the z -test for population proportions. For the other metrics, two-way ANOVAs were conducted to estimate group- and state-wise effects as well as their interaction. *Post hoc* comparisons were evaluated with a non-parametric t -test or a Tukey’s test.

Between-group comparisons for the modularity and overall connectivity, static and dynamic functional network analysis, dwell time, fraction time and occurrence rates were based only on participants who visited the respective state.

State-wise classification

Finally, group-wise analyses were complemented by a supervised binary classification approach to assess the potential of the static FC markers and the four dynamic FC states to discriminate between patients and controls. As previous work has suggested visual, fronto-parietal and DMN areas to represent the biologically relevant discriminatory features in anti-NMDA receptor encephalitis, these networks were considered as the set of input features.⁸ For the static design and each state, logistic regression models were trained on the z -scored FC indices to predict group status (anti-NMDA receptor encephalitis patients versus HC) in a leave-one-out cross-validation (LOOCV) scheme. To facilitate model sparsity and counteract overfitting, embedded feature selection was applied through L1 regularization. Hyperparameter optimization of the regularization strength λ was applied for each state-input matrix (observations-by-connectivity features) by searching a linearly spaced parameter grid that was identical for all four states. Selection probability of each feature was read out as the empirical rate of non-zeroed feature weights over all predictions within a state. Prediction performance was evaluated by standard confusion matrix

measures (i.e. true and false positive and negative rates and overall accuracy). Model training and prediction were implemented in Matlab (The MathWorks, Inc., Natick, MA, USA).

Data availability

The data that support the findings of this study are available upon reasonable request from the corresponding author. The code is available on GitHub (<https://github.com/nivons/statedynamicsNMDARE>).

Results

Functional network analysis

Static functional network connectivity analysis

We observed pairwise (component-to-component) differences in static FC between anti-NMDA receptor encephalitis patients and HC that clustered in the inter- and intra-connectivity of the DMN (Fig. 1 and Table 1). In line with previous studies,^{3,8} anti-NMDA receptor encephalitis patients showed decreased static connectivity between the hippocampus (HPC) and the medial prefrontal cortex (mPFC; $P_{\text{FDR}} < 0.05$). In addition, anti-NMDA receptor encephalitis patients exhibited significantly reduced DMN connectivity with the supplementary motor area, temporo-parieto-occipital junction (TPOJ), the parieto-occipital sulcus (POS) and the superior frontal gyrus (SFG) and increased FC with the orbito-frontal gyrus (OFG) ($P_{\text{uncorr}} < 0.001$). There was no significant difference between patients and controls in modularity ($\text{mean} \pm \text{SD}$: 0.35 ± 0.09 versus 0.33 ± 0.09 ; $t = -1.19$, $P = 0.12$) and overall connectivity (0.30 ± 0.05 versus 0.31 ± 0.07 ; $t = 0.63$, $P = 0.26$).

Following previous studies that found a correlation between the mPFC-hippocampal connection and disease severity variables,^{3,8} we conducted a *post hoc* correlation analysis (using Pearson's correlation coefficient) between these regions and disease severity at the time of scan (mRS). Higher mRS scores were associated with a reduced connectivity between the parahippocampal gyrus (PHG) and the mPFC ($r = -0.28$, $P = 0.040$), as well as with lower connectivity between the hippocampus and the mPFC ($r = -0.27$, $P = 0.05$).

Dynamic functional network connectivity analysis

K-means clustering identified four connectivity states for HC and anti-NMDA receptor encephalitis patients (Fig. 2). Group-wise mean connectivity and modularity for each state are shown in Fig. 3. Multiple regression models for modularity and overall connectivity yielded a significant effect for the state (modularity, $P < 0.001$; overall connectivity, $P < 0.001$), but not for group or interaction. The dominant State 1 closely resembled the static FC pattern ($r = 0.94$, Supplementary Table 14) with low overall connectivity and moderate modularity. States 2 and 3 were both characterized by high overall connectivity, while only State 2 had a

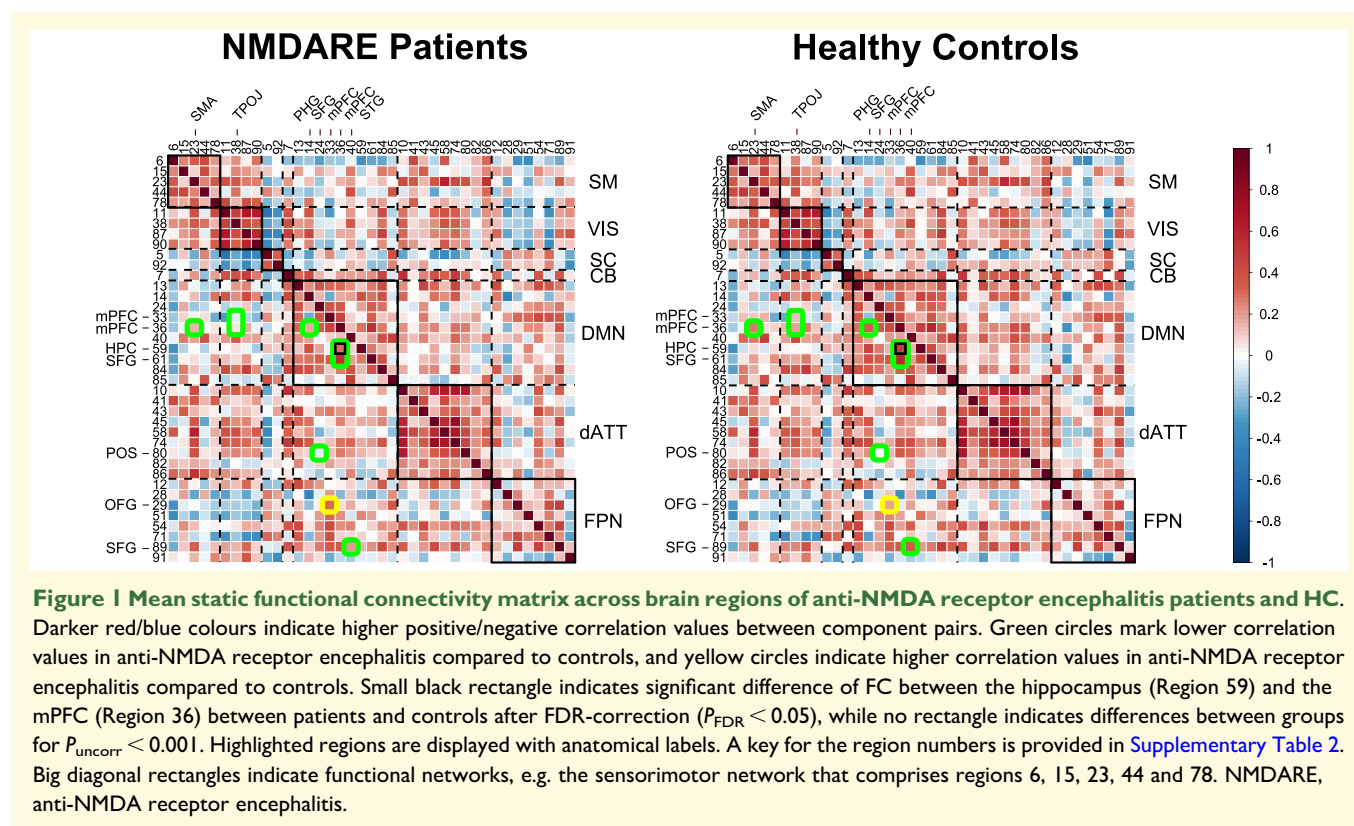
highly segregated structure (i.e. high modularity). In contrast to State 3, State 4 exhibited high modularity and low overall connectivity (Fig. 3, see Supplementary Tables 3–8 for detailed test statistics).

Anti-NMDA receptor encephalitis patients showed distinct FC alterations across the four connectivity states in comparison to controls (Fig. 2 and Table 2). As in the static FC group analysis, group differences comprised the DMN, VIS and FPN, but in a state-dependent fashion: in the static FC-resembling State 1, patients with anti-NMDA receptor encephalitis displayed decreased connectivity between the mPFC and the hippocampus, i.e. results very similar to the findings in the static FC analysis. The highly modular State 2 showed impaired connectivity between the mPFC and the angular gyrus (AG) as well as the parieto-occipital sulcus in patients. Furthermore, the inferior frontal gyrus (IFG) exhibited connectivity alterations with the putamen (bil.) and the visual cortex. Similarly, the densely connected/highly integrative State 3 was characterized by decreased connectivity from the IFG to the putamen. Additionally, connectivity between the TPOJ and the superior frontal gyrus was reduced in anti-NMDA receptor encephalitis patients compared to HC. For State 4, no significant alterations were observed after false discovery rate (FDR) correction.

Next, we obtained the correlation coefficient between all significant component pairs and disease severity (mRS at the time of scan) as well as disease duration (days in hospitalization): in the strongly segregated State 2, higher disease severity was significantly associated with a decrease in FC between mPFC and angular gyrus ($r = -0.37$, $P = 0.019$), while in the densely connected/highly integrative State 3, higher disease severity was significantly related to a decrease in connectivity between TPOJ and dorsolateral superior frontal gyrus ($r = -0.39$, $P = 0.046$). Due to the exploratory nature of the study, *post hoc* correlation analyses were not corrected for multiple comparisons.

State dynamics

In addition to state-wise connectivity patterns, we assessed state and group differences in dwell time, transition frequency, fraction time and occurrence rate using two-way ANOVAs. We found a significant state effect in *dwell times* ($P = 0.00021$): dwell times were higher for patients and controls in State 1 compared to States 2 ($T = -3.77$, $P = 0.0010$) and 3 ($T = -3.61$, $P = 0.0019$). Importantly, a significant group effect ($P = 0.010$) revealed a shift in dwell times between patients and controls: while patients showed lower dwell times in the dominant static FC-resembling State 1 ($P = 0.020$), they had higher dwell times in the strongly segregated State 2 compared to controls ($P = 0.032$; Fig. 4). Similarly, the model for *transition frequencies* yielded a significant effect for the group ($P = 0.044$) and state ($P < 0.001$). *Post hoc* group comparisons exhibited higher transition frequencies in patients between states with high and low overall connectivity, i.e. States 1 and 2 ($P = 0.043$), and between states with high and low across-



network connectivity, i.e. States 3 and 4 ($P = 0.0063$; [Fig. 4](#)), in comparison to controls. Furthermore, transitions from/to State 1 were significantly more frequent than transitions from States 2/3 to State 4 or vice versa. *Fraction time* differed across states ($P = 0.0023$), but not between groups ($P = 0.56$). A *post hoc* test revealed higher percentages of windows in State 1 compared to State 2 ($T = -3.23$, $P = 0.0077$) and 3 ($T = -3.02$, $P = 0.014$). *Occurrence rates* of dynamic FC states were similar in anti-NMDA receptor encephalitis patients and HC: the static FC-resembling State 1 showed the highest occurrence, followed by States 2 and 4; the lowest occurrence rates were observed for the densely connected/highly integrative State 3. Despite similar general occurrences, state-wise between-group proportion tests revealed that a higher number of patients visited the highly segregated State 2 compared to controls ($P = 0.019$), while the proportions were equal for both groups in States 1, 3 and 4. Detailed test statistics can be found in [Table 3](#) and [Supplementary Tables 9–13](#).

To identify a relationship between disease severity variables (i.e. acute days in hospitalization and mRS score at the time of scan) and dynamic metrics (i.e. dwell time and transition frequency), we conducted Pearson's correlation analyses between these variables. We found that increased transition frequency between States 1 and 2 was associated with disease severity at the time of scan ($r = 0.34$, $P = 0.012$). We further compared dwell time and transition frequency from patients with positive and negative schizophrenia-like psychiatric symptoms to those without

respective psychiatric symptoms. Here, patients with positive symptoms exhibited higher dwell times ($z = 2.07$, $P = 0.038$) in the highly segregated State 4 compared to those without positive symptoms. In contrast, patients with negative symptoms showed higher dwell times ($z = 2.02$, $P = 0.043$) in the densely connected/highly integrative State 3 compared to those without negative symptoms.

Classification analyses

Binary classification (anti-NMDA receptor encephalitis patients versus HC) based on static connectivity features yielded an overall prediction accuracy of 72%, with balanced feature distribution across the networks (see [Supplementary Fig. 3](#)). When dynamic connectivity features were considered, discriminatory power differed in a state-wise fashion. Prediction performance was lowest for the dominant, static FC-resembling State 1 (overall accuracy of 61.5%), intermediate and similar to model performance with static feature input for the modular-structured States 2 (72.6%) and 4 (70.8%), and highest for the least frequent and densely connected/highly integrative State 3 (78.6%; see [Supplementary Fig. 4](#) for the state-wise confusion matrices). Besides model evaluation outcomes, the feature selection frequencies over individual predictions in the LOOCV scheme also varied across states ([Fig. 5](#)). While States 1 and 3 yielded balanced selection rates over both across- and within-network connectivity features, States 2 and 4 showed fewer discriminatory features, and these were primarily across-network connections (FPN to VIS and DMN for State 2

Table 1. Test results of static functional network connectivity analysis

Regions	Network	Component #	P_{uncorr}	P_{FDR}	T	d
mPFC—hippocampus	DMN—DMN	36–59	<0.0001*	0.00024*	4.36	0.62
mPFC—SMA	DMN—SM	36–23	0.00092	0.15	3.30	0.44
mPFC—TPOJ	DMN—VIS	33–38	0.00084	0.15	3.26	0.54
mPFC—TPOJ	DMN—VIS	36–38	0.00061	0.15	3.40	0.45
mPFC—PHG	DMN—DMN	36–14	0.00016	0.12	3.85	0.55
SFG—POS	DMN—dATT	24–80	0.00072	0.15	3.29	0.52
mPFC—OFG	DMN—FPN	33–29	0.00043	0.15	−3.48	−0.37
mPFC—SFG	DMN—DMN	36–61	0.00087	0.15	3.27	0.40
STG—SFG	DMN—FPN	40–89	0.00057	0.15	3.24	0.49

Table includes component name, network assignment, number (#), t -value, P -value and effect size (d) of component pairs that are highlighted in Fig. 1.

*Significant after FDR-correction.

and DMN to VIS for State 4). Importantly, although some connectivity features were discriminatory across several states (e.g. component pairs 12–90 showed high selection frequency for States 1–3), the constellation of predictive features changed dynamically over connectivity states, emphasizing the uniqueness of each state.

Discussion

In this study, we applied dynamic FC analyses to characterize distinct connectivity patterns and temporal dynamics of network interactions in anti-NMDA receptor encephalitis. Investigating state-specific FC alterations, we found a marked impairment of FC between the hippocampus and the mPFC in the most visited, i.e. dominant state. This connectivity pattern closely mirrored observations in the static FC analysis and corroborated previous findings.^{3,8} Three additionally identified states showed connectivity alterations within the DMN and between frontal, visual and SB areas—findings that remained undetected in the static FC analysis. Investigation of state dynamics showed a systematic shift in dwell time from the dominant state to a strongly segregated state in patients. Likewise, negative and positive schizophrenia-like symptoms were associated with distinct patterns of state preference. In addition, an increased volatility of transitions between states with high and low overall connectivity and states with high and low segregation was observed in patients. These state dynamics were associated with disease severity. Finally, classification analyses revealed that discriminatory network features and predictive power varied dynamically across states, exceeding the discriminatory power of static FC analyses and yielding the highest prediction in a highly connected/highly integrated state. Our observations demonstrate the potential of time-resolved FC analysis for a better characterization of disease mechanisms involved in anti-NMDA receptor encephalitis.

Static functional network connectivity analysis

In line with previous studies, conventional static FC analyses showed impaired connectivity between the mPFC and the

hippocampus as well as altered connectivity patterns in frontal parts of the DMN.^{3,8} Indeed, the CA1 subregion of the hippocampus and the prefrontal cortex contains the highest density of NMDA receptors.²⁴ Converging observations of disrupted hippocampal–prefrontal connectivity are thus biologically plausible and point to a robust disease biomarker and potential treatment target in anti-NMDA receptor encephalitis. Furthermore, both brain regions are main components of the DMN and are involved in memory and executive functions^{25,26}—the two cognitive domains most frequently impaired in patients with anti-NMDA receptor encephalitis.^{4,6,27,28}

Dynamic functional network connectivity analysis

However, these findings are inherently limited to a static account of connectivity changes. Time-varying FC, in contrast, captures moment-to-moment changes in connectivity, reflecting a more physiologically plausible model of brain activity. One line of thought hypothesizes that the temporal variability of FC networks enables a systematic exploration of network configurations, which allows brain regions to dynamically (dis-)engage, and modulate changes in cognition and behaviour.²⁹ Dynamic state analysis as employed in this study represents a powerful tool to describe these dynamics and potential instabilities of this process.¹⁶

Indeed, state-wise group comparisons revealed connectivity differences between patients and controls in three out of four states. These differences were most pronounced in within- and across-network connectivity of the DMN and almost exclusively manifested as reduced connectivity strength in anti-NMDA receptor encephalitis.

State 1 represented the dominant state, i.e. the most visited state, the state in which participants remained longest and that was involved in most transitions. The connectivity pattern of State 1 was characterized by low overall connectivity and low segregation. Anti-NMDA receptor encephalitis patients showed a significantly impaired hippocampal–prefrontal connectivity in comparison to controls that closely resembled the pattern observed in current and previous static FC analyses.^{3,8} Thus, the connectivity pattern

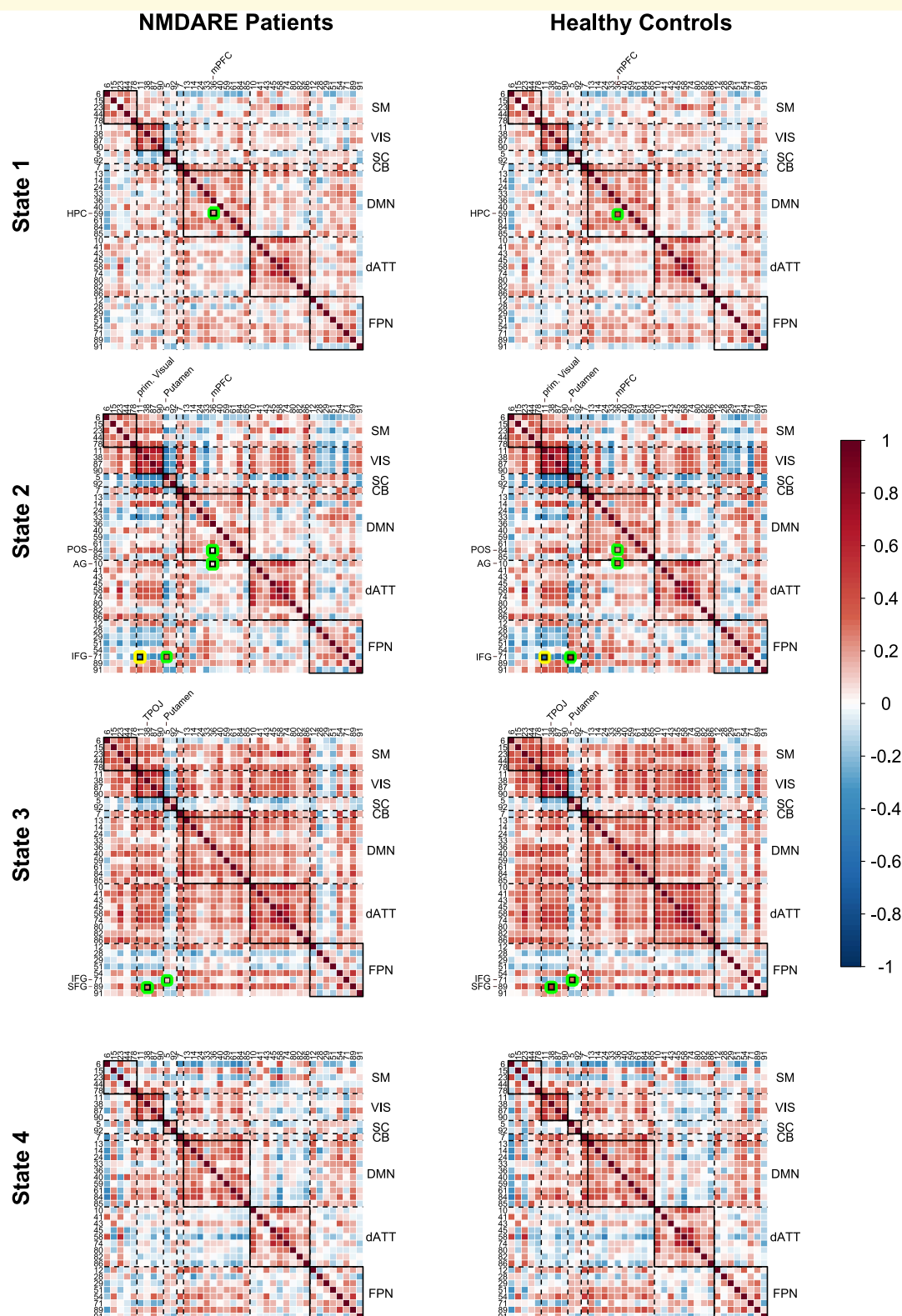


Figure 2 Dynamic functional network connectivity states for anti-NMDA receptor encephalitis patients and healthy controls. Darker red/blue colours indicate higher positive/negative correlation values between component pairs. Green circles mark lower correlation values in anti-NMDA receptor encephalitis compared to controls and yellow circles indicate higher correlation values in anti-NMDA receptor encephalitis compared to controls. Small black rectangles indicate significant differences of FC between patients and controls after FDR-correction ($P_{FDR} < 0.05$). Highlighted regions are displayed with anatomical labels. A key for the region numbers is provided in [Supplementary Table 2](#). Big diagonal black rectangles indicate functional networks, e.g. the sensorimotor network that comprises regions 6, 15, 23, 44 and 78. NMDARE, anti-NMDA receptor encephalitis.

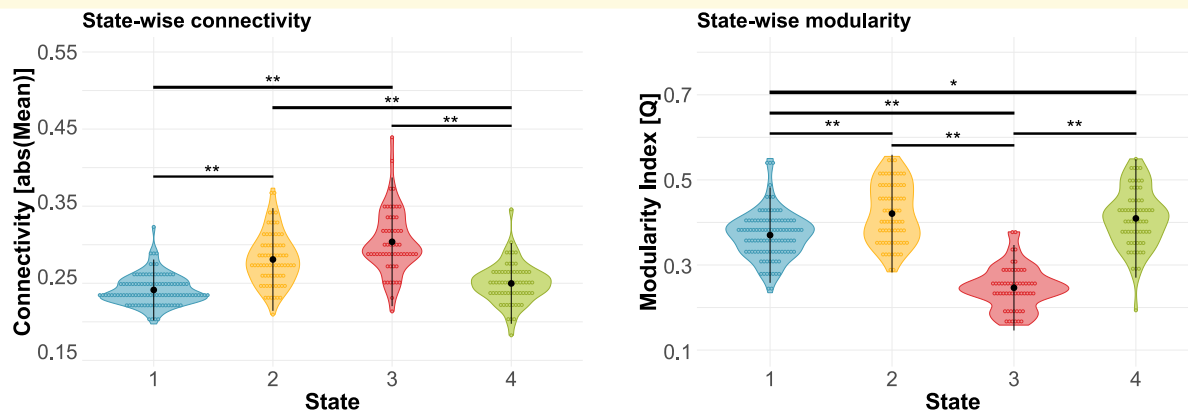


Figure 3 State-wise comparison of overall connectivity and modularity. In general, States 1 and 4 exhibited weak overall state connectivity compared to States 2 and 3. Segregation of functional networks, as measured with modularity, was highest in States 2 and 4, followed by State 1 and weakest in State 3. Black dots and vertical lines represent mean and standard deviation $**P < 0.001$ (Bonferroni-corrected). $*P < 0.01$ (Bonferroni-corrected). Detailed test statistics can be found in [Supplementary Tables 3–8](#).

in the dominant State 1 seems to drive findings of altered connectivity in conventional static FC analyses. In contrast, States 2–4 showed strikingly different features. FC alterations in States 2 and 3 went beyond the aggregated findings of the static analysis and revealed impaired connectivity between the mPFC and parieto-occipital areas, and between the IFG and the putamen (State 2). The latter is also present in State 3 along with impaired frontal-parietal connectivity.

Importantly, correlation analyses revealed that these dynamic FC alterations were associated with disease severity and disease duration, primarily involving mPFC connectivity and highlighting the clinical relevance of these findings. Together, these results disentangle state-specific connectivity patterns observed in conventional FC analyses and indicate the potential differential contribution of state-wise FC alterations to clinical symptoms and disease stages.

State dynamics

In addition to these alterations in large-scale connectivity patterns in different states, anti-NMDA receptor encephalitis patients showed distinct temporal properties with respect to connectivity states, i.e. different transition frequencies and dwell times in comparison to controls.

This involved a systematic shift in dwell time from the dominant State 1 to the segregated State 2, with patients nearly doubling their dwell time in State 2. Interestingly, recent evidence shows that successful working memory performance relies on increased network integration.³⁰ Prolonged dwelling in the segregated, less-integrated State 2 might thus be related to the frequently observed working memory deficits in anti-NMDA receptor encephalitis.⁴ Remarkably, patients who experienced positive schizophrenia-like symptoms spent more time in the highly segregated State 4, while those with negative symptoms increased their dwell time in the highly integrative State 3. These observations are consistent with recent studies in schizophrenia showing an increased modular network structure in patients.³¹

Additionally, patients showed an increase in transition frequencies between States 1 and 2 as well as between States 3 and 4. These transition frequency alterations were significantly correlated with disease severity, indicating that severe anti-NMDA receptor encephalitis disease courses are associated with more volatile transition dynamics, while state preference (i.e. dwell time) is not affected. The dynamic interplay between brain regions—in the sense of the flexible (dis-)engagement of functional links and state transitions—is critical to efficiently process internal and external stimuli and flexibly adapt behaviour. While state transitions are

Table 2. Test results of dynamic functional network connectivity analysis

	Regions	Network	Component #	P_{FDR}	T	d
State 1	mPFC—hippocampus	DMN—DMN	36–59	0.0016	4.01	0.60
State 2	prim. Visual—IFG	VIS—FPN	11–71	0.016	−3.80	−0.57
	Putamen—IFG	SC—FPN	5–71	0.016	4.09	0.56
	mPFC—angular gyrus	DMN—DMN	36–84	0.016	3.83	0.54
	mPFC—POS	DMN—dATT	36–10	0.016	4.06	0.79
State 3	TPOJ—SFG	VIS—FPN	38–89	0.00021	4.33	0.78
	Putamen—IFG	SC—FPN	5–71	0.041	3.99	0.69

Table includes component name, network assignment, number (#), t-value, P -value and effect size (d) of component pairs that are highlighted in [Fig. 2](#).

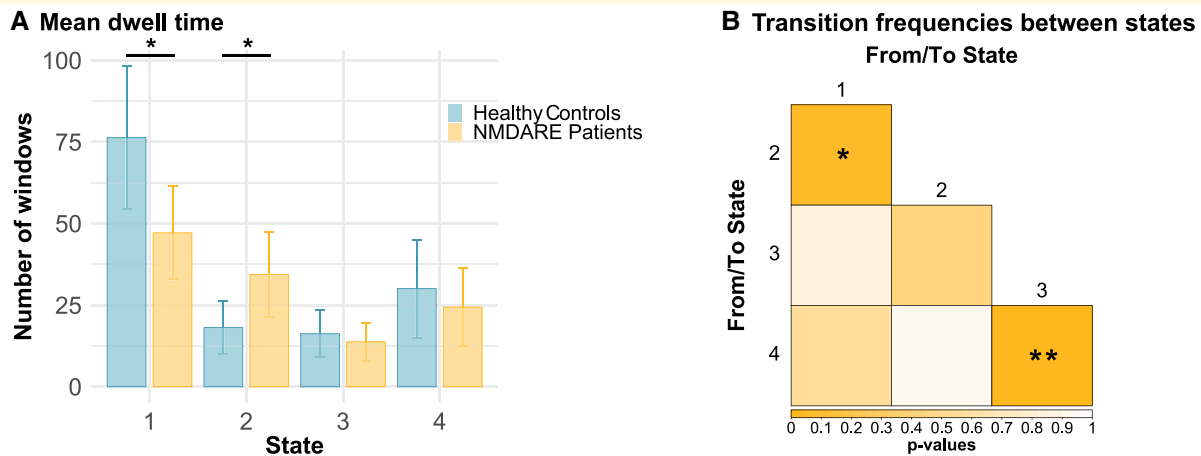


Figure 4 Group differences in state dynamics. (A) Group differences in average dwell time (in windows). Solid lines point to significant differences in *post hoc* testing between groups (non-parametric *t*-test, uncorrected). (B) Group differences in transition frequencies between states (*P*-values). For transition frequencies, the direction of transition was ignored. *Post hoc* group comparisons were calculated using a non-parametric *t*-test (uncorrected). **P* < 0.05; ***P* < 0.01. NMDARE, anti-NMDA receptor encephalitis.

thought to be generally important to explore different brain states in order to facilitate and enhance cognitive flexibility, overly unstable transition dynamics may be linked to deficiencies in the integration and stable representation of information.^{29,32} The imbalance of stability and volatility may, therefore, lead to impaired memory, perception or executive functions.^{33,34} These suggestive links between state dynamics and impaired cognitive performance in anti-NMDA receptor encephalitis require further detailed investigations in combined task-based and resting-state fMRI studies.³⁵

Relation to other brain disorders

Previous studies have applied dynamic FC analyses to brain disorders such as major depression, Alzheimer's disease or schizophrenia.^{12,13,15,36,37} In these studies—and those with

HC only¹⁶—the most visited state resembled the weakly connected dominant State 1 in the present study suggesting the brain's preference for a cost-efficient, energy-saving 'default' state.^{38,39} Moreover, patient groups showed characteristic changes in state dynamics, such as altered state occurrences, transition frequency or dwell times.^{12,13,36,37}

In patients with major depression, decreased variability in FC is the most prominent finding along with prolonged dwell times in the weakly connected dominant state.^{13,40–42} Changes in dynamic metrics were associated with sadness and disease severity and may mirror main symptoms including negative, slow and ruminative thinking.^{13,40}

A different pattern was found for patients with Alzheimer's disease. Similar to patients with anti-NMDA receptor encephalitis, state transitions are more volatile and patients tend to spend more time in less frequent,

Table 3. Group differences in dwell time (average number of windows), transition frequencies between states (absolute numbers) and fraction time (percentage).

	State	NMDARE patients (mean ± SD)	Healthy controls (mean ± SD)	<i>P</i> _{uncorr}	<i>d</i>
Dwell time	1	46.6 ± 53.8	75.7 ± 85.6	0.020*	0.43
	2	34.9 ± 49.9	17.6 ± 30.6	0.032*	−0.42
	3	14.2 ± 22.8	16.2 ± 28.0	0.21	0.22
	4	24.3 ± 45.0	30.3 ± 58.8	0.12	0.31
Transition frequency	1–2	1.3 ± 1.5	0.8 ± 1.37	0.043*	−0.34
	1–3	0.8 ± 1.4	0.8 ± 1.42	0.85	0.03
	1–4	1.3 ± 1.9	1.1 ± 1.95	0.55	−0.11
	2–3	0.5 ± 1.3	0.7 ± 1.31	0.44	0.14
	2–4	0.3 ± 0.8	0.3 ± 0.95	0.92	0.01
	3–4	0.3 ± 0.9	0.0 ± 0.13	0.0063*	−0.50
Fraction time	1	51.0 ± 33.1	54.7 ± 38.0	0.30	0.11
	2	31.5 ± 29.0	31.5 ± 25.8	0.48	0.01
	3	27.4 ± 27.7	32.3 ± 29.2	0.27	0.17
	4	32.8 ± 31.7	39.1 ± 33.9	0.22	0.20

Group differences were calculated using a two-sided non-parametric *t*-test. *P*-values and effect sizes (*d*) are shown. NMDARE, anti-NMDA receptor encephalitis.

**P* < 0.05 (uncorrected).

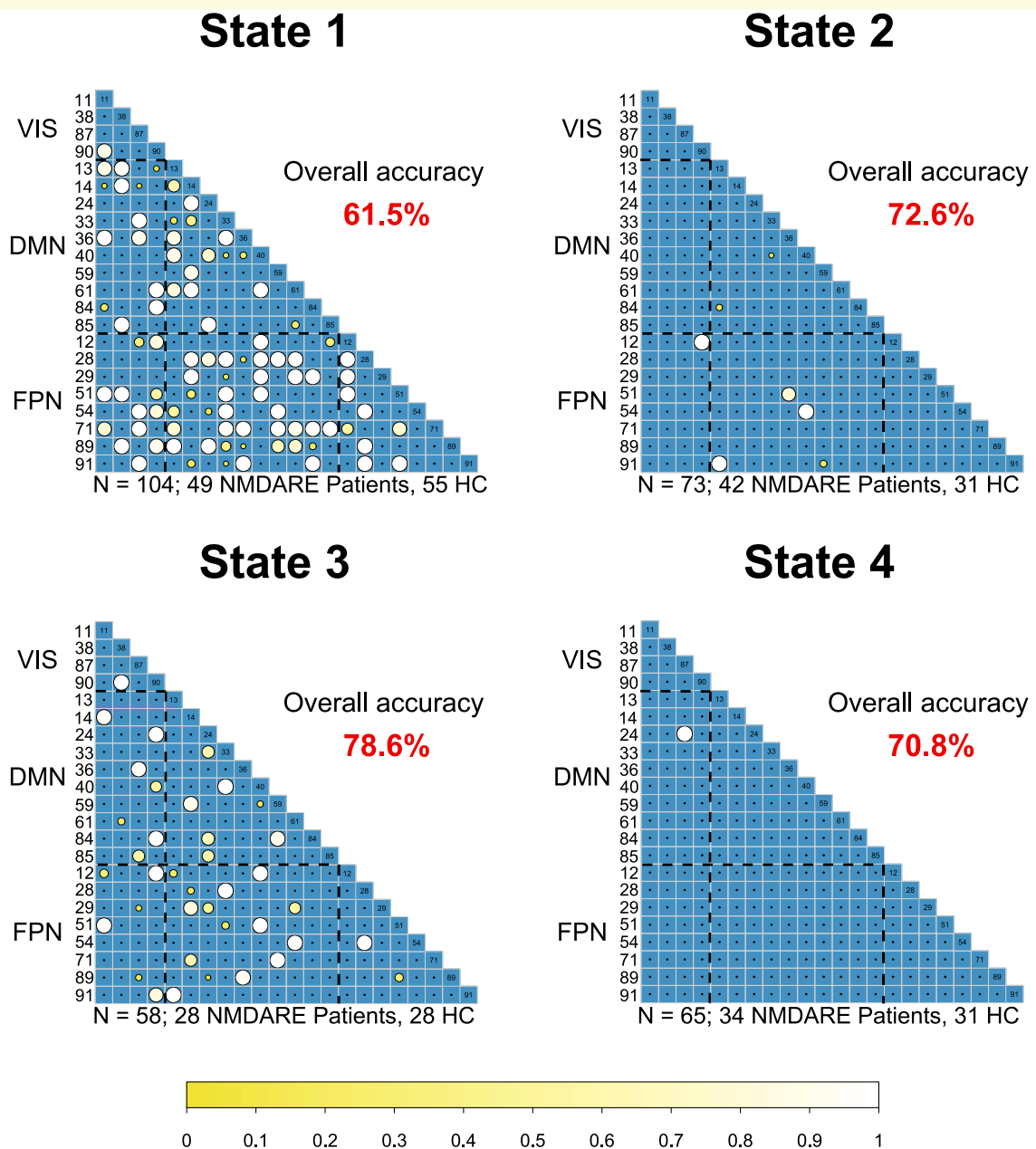


Figure 5 Feature selection matrices for state-wise predictions of group status (anti-NMDA receptor encephalitis patients versus healthy controls). The feature selection exceeding a minimum threshold at 10% of individuals within state predictions are displayed. Bigger and brighter circles indicate a higher selection rate. A key for the region numbers is provided in [Supplementary Table 2](#). NMDARE, anti-NMDA receptor encephalitis.

functionally segregated states as compared to HC.^{36,37} Interestingly, however, opposite results have also been reported,⁴³ potentially because dynamic connectivity pattern alterations change progressively across disease stages.

Furthermore, our results show a notable convergence with recent studies in patients with schizophrenia reporting a similarly marked shift in state preference¹² as well as increased overall transition frequencies,⁴⁴ and altered modular network structure.³¹ Given the considerable overlap in psychiatric symptoms in patients with schizophrenia and anti-NMDA receptor encephalitis^{45,46} and the glutamate

hypothesis positing NMDA receptor dysfunction as the pathophysiological basis for cognitive and psychiatric symptoms in schizophrenia,^{47,48} our findings raise the interesting possibility that the transdiagnostic psychopathological profile of both diseases⁴⁹ could be paralleled by a common set of dynamic network alterations.

Classification analyses

While our findings support the role of the hippocampus, the anterior DMN and frontal areas as potential connectivity

biomarkers in anti-NMDA receptor encephalitis, group-level analyses are not suited to estimate the discriminatory power of connectivity alterations or their value to predict disease severity.⁵⁰ To this end, we applied classification analyses based on logistic regression models to these data. Prediction performance and the set of selected network features were variable across the different connectivity states, indicating that discriminatory network constellations differ between states. Interestingly, the best performance (78.6% accuracy) was achieved in State 3, which showed the lowest overall occurrences but a highly integrative connectivity pattern. In contrast, static FC distinguished patients from controls with 72% accuracy. These results show that dynamic FC models can outperform static models and indicate the potential of spatiotemporal FC dynamics as prognostic biomarkers in anti-NMDA receptor encephalitis. However, further prospective studies are needed to identify biomarkers that can be used on the individual participant level and in clinical settings.

Limitations

Some limitations of the present study deserve mentioning. First, window-based approaches require the specification of windowing parameters and the optimal choices in this regard are an active area of research and debate.⁵¹ Second, a given window size may only capture a part of the dynamic nature of the human brain, as networks may reconfigure over different time scales even within the possible temporal spectrum of MRI signals.⁵¹ Lastly, for classification analyses, it is generally sensible to include large amounts of data.⁵⁰ While our study is based on a large study population in the light of the incidence of the disease, the sample sizes per state varied as not all participants visited all states.

Conclusions

Our analyses identified distinct brain states with characteristic patterns of FC alterations and shifted temporal dynamics in patients with anti-NMDA receptor encephalitis that remained undetected in conventional static analyses. Critically, dynamic FC measures correlated with disease severity and psychiatric symptoms, suggesting that altered resting-state dynamics carry meaningful clinical information about anti-NMDA receptor encephalitis. Given converging findings in other neuropsychiatric diseases, time-resolved FC analysis holds promise for an improved characterization and understanding of brain functioning in these disorders.

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N.v.S. designed the study, conducted the static and dynamic functional network connectivity analysis, led the writing of the manuscript and produced the figures. S.K. implemented the classification analysis. S.K. and C.F. (principal investigator) significantly contributed to the design and

interpretation of the analysis and writing. N.v.S., J.H. and C.F. rated the components from the group ICA. J.H., F.P., H.P. and C.F. were involved in conceiving/conducting the cohort study and data collection. All authors edited and revised the manuscript. The graphical abstract was created with BioRender.com.

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Competing interests

N.v.S., S.K., J.H., H.P. and C.F. have nothing to disclose. F.P. reports grants and personal fees from Bayer, Biogen Idec, Merck Serono, Alexion, Guthy Jackson Foundation, Viela Bio, Novartis, Roche and Sanofi Genzyme. F.P. is the Academic Editor of *Plos One* and Associate Editor of *Neurology*, *Neuroimmunology & Neuroinflammation*. F.P. receives personal fees from Mitsubishi Tanabe PC (MTPC), and from UCB, outside the submitted work.

Supplementary material

[Supplementary material](#) is available at *Brain Communications* online.

References

1. Dalmau J, Lancaster E, Martinez-Hernandez E, Rosenfeld MR, Balice-Gordon R. Clinical experience and laboratory investigations in patients with anti-NMDAR encephalitis. *Lancet Neurol*. 2011; 10(1):63–74.
2. Kayser MS, Dalmau J. Anti-NMDA receptor encephalitis, autoimmunity, and psychosis. *Schizophr Res*. 2016;176(1):36–40.
3. Finke C, Kopp UA, Scheel M, et al. Functional and structural brain changes in anti-N-methyl-D-aspartate receptor encephalitis. *Ann Neurol*. 2013;24(2):284–296.
4. Finke C, Kopp UA, Prüss H, Dalmau J, Wandinger KP, Ploner CJ. Cognitive deficits following anti-NMDA receptor encephalitis. *J Neurol Neurosurg Psychiatry*. 2012;83(2):195–198.
5. Graus F, Titulaer MJ, Balu R, et al. A clinical approach to diagnosis of autoimmune encephalitis. *Lancet Neurol*. 2016;15(4):391–404.
6. Heine J, Kopp UA, Klag J, Ploner CJ, Prüss H, Finke C. Long-term cognitive outcome in anti-NMDA receptor encephalitis. *Ann Neurol*. 2021;90:949–961.

7. Heine J, Prüss H, Bartsch T, Ploner CJ, Paul F, Finke C. Imaging of autoimmune encephalitis – relevance for clinical practice and hippocampal function. *Neuroscience*. 2015;309:68–83.
8. Peer M, Prüss H, Ben-Dayan I, Paul F, Arzy S, Finke C. Functional connectivity of large-scale brain networks in patients with anti-NMDA receptor encephalitis: An observational study. *Lancet Psychiatry*. 2017;4(10):768–774.
9. Calhoun VD, Miller R, Pearlson G, Adalı T. The chronnectome: time-varying connectivity networks as the next frontier in fMRI data discovery. *Neuron*. 2014;84(2):262–274.
10. Hutchison RM, Womelsdorf T, Allen EA, et al. Dynamic functional connectivity: Promise, issues, and interpretations. *NeuroImage*. 2013;80:360–378.
11. Chang C, Glover GH. Time–frequency dynamics of resting-state brain connectivity measured with fMRI. *NeuroImage*. 2010;50(1):81–98.
12. Damaraju E, Allen EA, Belger A, et al. Dynamic functional connectivity analysis reveals transient states of dysconnectivity in schizophrenia. *NeuroImage Clin*. 2014;5:298–308.
13. Demirtaş M, Tornador C, Falcón C, et al. Dynamic functional connectivity reveals altered variability in functional connectivity among patients with major depressive disorder. *Hum Brain Mapp*. 2016;37(8):2918–2930.
14. Jones DT, Vemuri P, Murphy MC, et al. Non-stationarity in the “resting brain’s” modular architecture. *PLoS One*. 2012;7(6):e39731.
15. Bonkhoff AK, Espinoza FA, Gazula H, et al. Acute ischaemic stroke alters the brain’s preference for distinct dynamic connectivity states. *Brain*. 2020;143(5):1525–1540.
16. Allen EA, Damaraju E, Plis SM, Erhardt EB, Eichele T, Calhoun VD. Tracking whole-brain connectivity dynamics in the resting state. *Cereb Cortex*. 2014;24(3):663–676.
17. Calhoun VD, Adalı T, Pearlson GD, Pekar JJ. A method for making group inferences from functional MRI data using independent component analysis. *Hum Brain Mapp*. 2001;14(3):140–151.
18. Himberg J, Hyvarinen A. Icaso: Software for investigating the reliability of ICA estimates by clustering and visualization. In: IEEE XIII Workshop on Neural Networks for Signal Processing. IEEE. 2003.
19. Du Y, Fan Y. Group information guided ICA for fMRI data analysis. *NeuroImage*. 2013;69:157–197.
20. Thomas Yeo BT, Krienen FM, Sepulcre J, et al. The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *J Neurophysiol*. 2011;106(3):1125–1165.
21. Blondel VD, Guillaume JL, Lambiotte R, Lefebvre E. Fast unfolding of communities in large networks. *J Stat Mech Theory Exp*. 2008(10):P10008.
22. Rubinov M, Sporns O. Complex network measures of brain connectivity: Uses and interpretations. *NeuroImage*. 2010;52(3):1059–1069.
23. Glerean E, Pan RK, Salmi J, et al. Reorganization of functionally connected brain subnetworks in high-functioning autism. *Hum Brain Mapp*. 2016;37(3):1066–1079.
24. Monaghan DT, Cotman CW. Distribution of N-methyl-D-aspartate-sensitive L-[3H]glutamate-binding sites in rat brain. *J Neurosci*. 1985;5(11):2909–2919.
25. Miller EK, Cohen JD. An integrative theory of prefrontal cortex function. *Annu Rev Neurosci*. 2001;24(1):167–202.
26. Barbosa J, Stein H, Martinez RL, et al. Interplay between persistent activity and activity-silent dynamics in the prefrontal cortex underlies serial biases in working memory. *Nat Neurosci*. 2020;23(8):1016–1024.
27. McKeon GL, Robinson GA, Ryan AE, et al. Cognitive outcomes following anti-N-methyl-D-aspartate receptor encephalitis: A systematic review. *J Clin Exp Neuropsychol*. 2018;40(3):234–252.
28. Gibson LL, McKeever A, Coutinho E, Finke C, Pollak TA. Cognitive impact of neuronal antibodies: Encephalitis and beyond. *Transl Psychiatry*. 2020;10(1):304.
29. Deco G, Jirsa VK, McIntosh AR. Emerging concepts for the dynamical organization of resting-state activity in the brain. *Nat Rev Neurosci*. 2011;12(1):43–56.
30. Cohen JR, D’Esposito M. The segregation and integration of distinct brain networks and their relationship to cognition. *J Neurosci*. 2016;36(48):12083–12094.
31. Alexander-Bloch AF, Gogtay N, Meunier D, et al. Disrupted modularity and local connectivity of brain functional networks in childhood-onset schizophrenia. *Front Syst Neurosci*. 2010;4:147.
32. Li L, Lu B, Yan CG. Stability of dynamic functional architecture differs between brain networks and states. *NeuroImage*. 2020;216:116230.
33. Braun U, Schäfer A, Walter H, et al. Dynamic reconfiguration of frontal brain networks during executive cognition in humans. *Proc Natl Acad Sci USA*. 2015;112(37):11678–11683.
34. Sadaghiani S, Poline JB, Kleinschmidt A, D’Esposito M. Ongoing dynamics in large-scale functional connectivity predict perception. *Proc Natl Acad Sci USA*. 2015;112(27):8463–8468.
35. Lorenz R, Johal M, Dick F, Hampshire A, Leech R, Geranmayeh F. A Bayesian optimization approach for rapidly mapping residual network function in stroke. *Brain*. 2021;144(7):2120–2134.
36. Fu Z, Caprihan A, Chen J, et al. Altered static and dynamic functional network connectivity in Alzheimer’s disease and subcortical ischemic vascular disease: shared and specific brain connectivity abnormalities. *Hum Brain Mapp*. 2019;40(11):3203–3221.
37. Gu Y, Lin Y, Huang L, et al. Abnormal dynamic functional connectivity in Alzheimer’s disease. *CNS Neurosci Ther*. 2020;26(9):962–971.
38. Fornito A, Zalesky A, Bassett DS, et al. Genetic influences on cost-efficient organization of human cortical functional networks. *J Neurosci*. 2011;31(9):3261–3270.
39. Krohn S, von Schwanenflug N, Waschke L, et al. A spatiotemporal complexity architecture of human brain activity. *Biorxiv*. 2021. doi:10.1101/2021.06.04.446948.
40. Marchitelli R, Paillère-Martinot M-L, Bourvis N, et al. Dynamic functional connectivity in adolescence-onset major depression: Relationships with severity and symptom dimensions. *Biol Psychiatry Cogn Neurosci Neuroimaging*. 2021:S2451902221001439.
41. Kaiser RH, Whitfield-Gabrieli S, Dillon DG, et al. Dynamic resting-state functional connectivity in major depression. *Neuropsychopharmacology*. 2016;41(7):1822–1830.
42. Yao Z, Shi J, Zhang Z, et al. Altered dynamic functional connectivity in weakly-connected state in major depressive disorder. *Clin Neurophysiol*. 2019;130(11):2096–2104.
43. Schumacher J, Peraza LR, Firbank M, et al. Dynamic functional connectivity changes in dementia with Lewy bodies and Alzheimer’s disease. *NeuroImage Clin*. 2019;22:101812.
44. Rashid B, Damaraju E, Pearlson GD, Calhoun VD. Dynamic connectivity states estimated from resting fMRI identify differences among Schizophrenia, bipolar disorder, and healthy control subjects. *Front Hum Neurosci*. 2014;8:897.
45. Al-Diwani A, Handel A, Townsend L, et al. The psychopathology of NMDAR-antibody encephalitis in adults: A systematic review and phenotypic analysis of individual patient data. *Lancet Psychiatry*. 2019;6(3):235–246.
46. Gibson LL, Pollak TA, Blackman G, Thornton M, Moran N, David AS. The psychiatric phenotype of anti-NMDA receptor encephalitis. *J Neuropsychiatry Clin Neurosci*. 2019;31(1):70–79.
47. Moghaddam B, Javitt D. From revolution to evolution: The glutamate hypothesis of schizophrenia and its implication for treatment. *Neuropsychopharmacology*. 2012;37(1):4–15.
48. Stein H, Barbosa J, Rosa-Justicia M, et al. Reduced serial dependence suggests deficits in synaptic potentiation in anti-NMDAR encephalitis and schizophrenia. *Nat Commun*. 2020;11(1):4250.
49. Finke C. A transdiagnostic pattern of psychiatric symptoms in autoimmune encephalitis. *Lancet Psychiatry*. 2019;6(3):191–193.
50. Arbabshirani MR, Plis S, Sui J, Calhoun VD. Single subject prediction of brain disorders in neuroimaging: Promises and pitfalls. *NeuroImage*. 2017;145:137–165.
51. Lurie DJ, Kessler D, Bassett DS, et al. Questions and controversies in the study of time-varying functional connectivity in resting fMRI. *Netw Neurosci*. 2020;4(1):30–69.